Full Research Paper

Photoresist Derived Carbon for Growth and Differentiation of Neuronal Cells

Hong Zhou^{1,*}, Anju Gupta¹, Tie Zou² and Jianhua Zhou²

Worcester Polytechnic Institute, Department of Chemical Engineering, 100 Institute Road,
 Worcester, MA 01609, USA
 University of Massachusetts, Medical School, Department of Medicine, 55 Lake Avenue North,

Worcester, MA 01655, USA

* Author to whom correspondence should be addressed; E-mail: szhou@wpi.edu

Received: 12 June 2007; in revised form: 17 July 2007 / Accepted: 27 July 2007 / Published: 27 August 2007

Abstract: Apoptosis or necrosis of neurons in the central nervous system (CNS) is the hallmark of many neurodegenerative diseases and Traumatic Brain Injury (TBI). The inability to regenerate in CNS offers little hope for naturally repairing the damaged neurons. However, with the rapid development of new technologies, regenerative medicine offers great promises to patients with these disorders. Among many events for further advancement of regenerative medicine, extracellular matrix (ECM) plays a critical role for cellular migration and differentiation. To develop a biocompatible and electrically conductive substrate that can be potentially used to promote growth and regeneration of neurons and to record intracellular and multisite signals from brain as a probe, a polymeric precursor - SPR 220.7 was fabricated by pyrolysis at temperatures higher than 700 °C. Human Neuroblastoma cells - SK-N-MC, SY5Y, mouse teratocarcinoma cells P-19 and rat PC12 cells were found to attach and proliferate on photoresist derived carbon film. Significantly, neuronal differentiation of PC12 cells induced by NGF was demonstrated by observing cell shape and size, and measuring the length of neurites under SEM. Our results indicated that fabricated carbon could potentially be explored in regenerative medicine for promoting neuronal growth and differentiation in CNS with neurodegeneration.

Keywords: Cell adhesion, carbon, nerve growth factor, nerve regeneration, scanning electron microscope

1. Introduction

Millions of lives are influenced by loss of neuronal function as a consequence of neurodegeneration or injury to the neuronal pathway of the central or peripheral nervous system. Neurons have the ability to repair and regenerate in case of minimal damages. But, if major damage occurs to the peripheral and central nervous systems, the neurons fail to restore themselves leading to a loss of memory, impaired sensory responses, muscle disfunctioning. Current efforts at solving this problem include nerve grafting and surgical suturing. These procedures are however limited by the availability of donor tissue, donor site morbidity, multiple surgeries and partial recovery [1].

Tissue engineering offers various engineered biodegradable and non-biodegradable templates for regeneration of severed neurons. These engineered constructs are a promising alternative due to their mechanical strength, biocompatibility and chemical inertness. A variety of natural materials such as laminin, fibronectin and collagen are employed to improve the efficacy of these substrates [2-4]. However these materials induce undesirable immune response and lack mechanical stability.

The need of mechanically stable neural implant materials led researchers to explore the possibility of employing various metals and non-metals for nerve regeneration purposes. Till now, silicon is being widely explored for the continuous monitoring, diagnosis and regeneration of neurons. Silicone tubes have been used for nerve restoration applications. They are non-biodegradable and impermeable to large molecules and create an isolated environment for nerve regeneration [5] Researchers have successfully shown the organization of neural networks on silicone tubes functionalized with laminin, collagen and fibronectin gels. Fromherz et al have been working on electrical interfacing between the individual nerve cells and have been working to control the mechanical and electrical quality of cell-semiconductor contact and signal processing between neurons [6]. However, the non-biodegradable silicon imparts inflexibility and induces foreign body reaction resulting from excessive scar tissue.

Lack of sufficient bonding of silicon implant to desirable surrounding tissue and lack of inherent flexibility, mechanical stability and electrical conductivity has led investigations of novel biomaterials that can overcome the limitations of synthetic implant devices. There has been growing interest to use carbon for biomedical applications. Carbon, especially in its fiber form, has been successfully used in the orthopedic and neural implants due to its composition, high aspect ratio, electrical and physical properties [7]. Previous studies have provided evidence that carbon fibers possess ability to be functionalized with biomolecules. This has made them successful candidates to form scaffolds to support neuron hybrids. Zhang et.al have demonstrated the capability of functionalized vertical nanotube arrays as support platform for guiding neurite growth and forming synaptic ally communicative networks [8]. Pyrolzed carbon is also being investigated for its applications in artificial heart valves due to its ability to maintain a coherent interface with living tissue and its ability of being non-thrombogenic in blood [9-10].

In the present work, we investigated the potentiality of carbon as a resultant of pyrolysis of polymeric precursor- SPR 220.7 for *in vivo* applications by culturing several human and rodent neuronal cells lines including neuroblastoma (SK-N-MC, SY5Y), carcinoma (P-19), and PC-12 (rat pheochromocytoma) cells *in vitro*. We show the successful growth and proliferation of these cell lines on photoresist derived carbon films that were not functionalized with naturally occurring protein or synthetically modified biopolymers. More importantly, we demonstrated that PC12 cells, a model

system for differentiation studies [13], can be induced to differentiate on carbon surface when subjected to differentiation-inducing substance NGF. One advantage of carbon material without functionalized with other biomolecules is that it would considerably reduce the undesirable immune response, if used in *vivo*. Other advantages of these carbon devices, derived from polymeric precursor, include excellent biocompatibility, wide electrochemical stability, and availability in high purity, reproducibility, chemical inertness, good thermal conductivity, dimensional and mechanical permanence [11-12]. Therefore, our results present evidence for further substantiation.

2. Materials and Methods

2.1 Fabrication of Carbon substrate

Carbon was derived from pyrolysis of photoresist coated on silicon wafer. A 2" diameter silicon wafer is cut into numerous chips of approximate length 15.6mm. Silicon chips were washed with 70% ethanol and then air dried. A clean silicon chip was placed in the spin coater. A layer of positive photoresist SPR 220-7.0 was applied to the silicon chip manually. The spin coater was run at 300 revolutions per minute (rpm) for 3 seconds to spread the photoresist on the wafer then run at 3000 rpm for 30 sec to fully situate the photoresist on the silicon chip. The photoresist coating process was repeated four times to ensure that the desired thickness range had been reached. Following the four coats, photoresist coated silicon chip was placed on a hot plate set at 95 °C for five minutes and was left to cool naturally to room temperature.

The chip was placed in a Nitrogen gas atmosphere. The gas atmosphere must be completely free of oxygen. The sample was heated at a rate of 10 °C per minute until the desired maximum temperature (700 °C to 1100 °C) had been reached. Once at the desired maximum temperature, the sample remained under heat at that temperature for one hour. The chip is allowed to cool in the nitrogen environment. Once at room temperature, the chip with a layer of carbon was ready to reenter an oxygenated atmosphere [11-12].

2.2 Cell Culture

Carbon chips were placed into wells of 6-well plate, washed with 70% v/v ethanol and sterilized under ultraviolet radiation for 45 minutes.

The rat pheochromocytoma PC12 cells were cultured in DMEM high glucose medium supplemented with 5% of FBS and 10% of Horse serum. The cells were induced to differentiate in DMEM high glucose medium (Gibco-11495) with 100 ng/mL of Nerve Growth Factor (Gibco 13257-019).

Human neuroblastoma cell lines (SK-N-MC, SY5Y), mouse teratocarcinoma cell line (P-19), were maintained in DMEM high glucose medium (Gibco 11495) supplemented with 10% fetal bovine serum (Gibco 26140-079) and penicillin-streptomycin (Gibco 15140-122). The cells were incubated at 37 °C with 5% CO₂ in cell culture dishes. The cells were removed from the cell culture dish with 0.25% trypsin EDTA (Gibco-25200). Removed cells were centrifuged at 1000 rpm for 5 minutes. The pellet was suspended with fresh medium, and counted via a haemocytometer. Approximately 100,000 cells were transferred to the sterilized carbon chip placed in wells of 24-well cell culture plate.

2.3 Scanning Electron Microscopy

Differentiated and undifferentiated cells on photoresist derived carbon were fixed by immersion in 2.5% (v/v) glutaraldehyde in 0.5 M Na cacodylate-HCl buffer (pH 7.2) for 1 hr at room temperature. The fixed samples were washed three times in the same buffer. Following the third wash the cells were post fixed for 1 hr in 1% osmium tetroxide (w/v) in the same buffer, washed three more times in the same buffer and left overnight at 4 °C in fresh buffer. The next morning the samples were dehydrated through a graded series of ethanol to 10% and then Critical Point Dried in liquid CO₂.

The carbon chips with the cells attached on the surface were affixed to aluminum SEM studs and sputter coated with Au/Pd (80/20). The specimens were then examined using an ETEC autoscan scanning electron microscope at 20 kV accelerating voltage [14].

3. Results

3.1 Carbon substrate characterization

The scanning electron microscopy (SEM) studies (Figure 1) showed that the photoresist derived carbon film had thickness of 10 μ m, with no porosity at several high magnifications. Atomic force microscopy (AFM) reports the films having a relatively smooth surface with an estimated root mean square (rms) roughness of 2 nm (Figure 2). X-ray diffraction revealed the graphitic nature of the carbon film (Figure 3).



Figure 1. SEM Images of Carbon Substrate.



Figure 2. Atomic Force Microscopic Image of Carbon Substrate.



Figure 3. X-Ray Diffraction Analysis of the Carbon substrate.

3.2 Cell adhesion

3.2.1 SK-N-MC, SY5Y, P-19 Cell adhesion

Different human and mouse cells were tested for their cytocompatibility with the unfunctionlized carbon substrate. Human neuroblastoma, SK-N-MC cells exhibit excellent adhesion even on untreated surfaces. Figure 4A presents the scanning electron microscope images of neuroblastoma cells cultured on the carbon template at a concentration of 3×10^5 cells/mL. Within 2 days of cell culturing, the surface of the template was observed to be covered entirely with cells. After 4 days of culturing cells started growing on top each other. Based on these observations, we conclude that cell growth rate on carbon surface is reasonable good. Another type of human neuroblastoma cells-SY5Y was also tested

to confirm the affinity of neuroblastoma cells to unfunctionalized photoresist derived carbon. Figure 4B presents the growth and proliferation of SY5Y cells cultured on carbon template and observed for 4 days. We also investigated mouse teratocarcinoma – P19 cells, Figure 4C represents the scanning electron microscope images of P19 cells fixed after 3 days. Cells were grown at a concentration of 2×10^4 cells/mL to avoid excessive populating of cells, as P19 cells are known to grow faster, absorbing all the nutrients from cell culture medium, leaving the medium acidic, resulting in early cell death.



Figure 4. Growth of neuronal cell lines on Carbon. A: SKN-MC cells; B: SY5Y cells; C: P19 cells.

3.2.2 PC 12 Cell Differentiation

Scanning electron micrographs of PC12 cells differentiation observed at the 1, 2, 3, 4 day time points are shown in Figure 5. Neurite outgrowth was observed after 24 hours of nerve growth factor injection. Cells tend to become less adhesive due to the growing tension in the neurite that connects the cells. This tensile force dominates the adhesion force causing looser contact with the substrate. However, cells grown on photoresist derived carbon remained on the substrate even after four days and extending to more than hundred microns to reach to the distant cells. Differences in neurite growth were quantified by measuring neurite length, the number of neuritis emanating per cell (Table 1). Neurites emerging from cells grown on carbon were significantly longer than neurites emerging from

control cells (on coated glass) (Figure 6) (Table 1). All these experiments were repeated at least three times and the number of neurites per cell and the average neurite length were quantitated from multiples cells (> 10) for each experiment. Our results consistently showed that carbon surface promoted PC12 cells differentiation after NGF treatment.



Figure 5. PC12 cells were induced to differentiate after NGF treatment A: 1 day; B: 2days; C: 3 days; D: 4 Days.

Table 1. Average values for measurements of neurite growth for differentiated PC12 cells cultured onPhotoresist derived carbon and Poly-l-Lysine coated glass (control).

	Photoresist derived carbon		Poly-L-lysine coated glass	
Time period	$L_{ m Neurite}$ (μ m)	N _{Neurite} (per cell)	L_{Neurite} (μ m)	N _{Neurite} (per cell)
Day 1	20	2	15	1
Day 2	40	5	30	2
Day 3	50	6	40	4
Day 4	100	6	60	5



Figure 6. Length of Neurite as a function of time.

4. Discussion

Thousands of lives are affected by peripheral nerve injuries and impaired central nervous system (CNS) resulting in painful neuropathies and accompanying malfunctioning of other body parts. Limitations of current strategies - suturing and grafting call for new approaches to tackle this issue. Several metals and ceramics are being employed in the field of neural implants for regeneration of severed neurons. Carbon in its fibrous form, functionalized with poly-l-lysine is widely used in the field of implant devices due to its aberrant mechanical and chemical properties. Tissue engineers have explored modifications of prosthetic devices such as natural protein coatings, chemical surface modifications and combination of polymers to increase the cell affinity of present implantable devices. The current study presented early stage investigations on a novel material that could potentially anchor different types of neuronal cells with varying adhesion properties in the field of neural implants. This carbon was synthesized by pyrolyzing a polymeric precursor - SPR 220.7. Scanning electron microscopy and atomic force microscopy analysis showed the surface to be very smooth. Human neuroblastoma - SK-N-MC and SY5Y cells and rat carcinoma - P19 cells showed growth and proliferation. We also investigated the response of rat pheochromocytoma -PC12 cells, a cell line known to have poor adhesion and requireing anchoring extra cellular matrix. We found that PC12 cells only not grew on carbon surface but also could be induced to differentiate by nerve growth factor. Interestingly, our results indicate that our fabricated carbon surface promoted PC12 differentiation.

5. Conclusion and Future Work

Conducted study provides the first implication that photoresist derived carbon may be explored as one of the options for promoting initial cell response that may lead to the future design of neural implants. The work presented in this paper demonstrates support for neural cell differentiation. The results represented meet the parameters for further investigation of photoresist derived carbon as a neural probe.

Topography of the substrate plays a vital role in determining cell response of cells to a structure. We can take the advantage of using photoresists as the starting material for carbon template, as the photoresists can be patterned by photolithography techniques. Once cells have been plated onto carbon structure in a specific pattern, we can selectively eliminate cells from the established network and study how cells reconnect after injury.

The ability to grow cultured neurons in a specific pattern and be able to record electrical activity will open up the area of study in neuronal networks and function. It would be then possible to record the extracellular potential from a cell body or the firing of an individual fiber to the outstanding electrical properties of photoresist derived carbon.

Acknowledgements

The authors would like to thank Dr. Gregory Hendricks, Manager, Core Electron Microscopy Facility, and University of Massachusetts Medical School for his contribution concerning the imaging of cultured neurons on photoresist derived carbon substrate.

References

- 1. Evans, G.R. Challenges to Nerve Regeneration. Semin. Surf. Oncol. 2000, 19, 312-318.
- 2. Hubbell, J.A. Bioactive Biomaterials. Curr. Opin. Biotechnol. 1999, 10(2), 123-129.
- 3. Massia, S.P.; Hubbell, J.A. An RGD spacing of 440 nm is sufficient for integrin $\alpha_{\varpi}\beta_{3-}$ mediated fibroblast spreading and 140 nm for local contact and stress fiber formation. *J. Cell Biol.* **1991**, *114*, 1089-1100.
- 4. Massia, S.P.; Rao, S.; Hubbell, J.A. Covalently immobilized laminin peptide Tyr-IIe-Gly-Ser-Arg (YIGSR) supports cell spreading and colocalization of the 67-kilodalton laminin receptor with alpha-actinin and vinculin. *J. Biol. Chem.* **1993**, *268*, 8053–8059.
- 5. Chen, Y.S; Hsieh, C.L.; Tsai, C.C; Chen, T.H.; Cheng, W.C.; Hu, C.L.; Yao, C.H. Peripheral Nerve Regeneration using Silicone Rubber Chambers Filled with Collagen, Laminin and Fibronectin. *Biomaterials* **2000**, *21*, 1541-1547.
- 6. Fromherz, P. Electrical Interfacing of Nerve Cells and Semiconductor Chips. *ChemPhyChem* **2002**, *3*(*3*), 276-284.
- 7. Webster, T.J.; Waid, M.C.; McKenzie, J.L.; Price, R.L.; Ejiofor, J.U. Nano-biotechnology: carbon nanofibres as improved neural and orthopaedic implants. *Nanotechnology*. **2004**, *15*(*1*), 48-54.
- 8. Zhang. X.; Prasad, S.; Niyogi, S.; Morgan, A.; Ozkan, M.; Ozkan, C.S. Guided neurite growth on patterned carbon nanotubes. *Sensor. Actuat. B-Chem.* **2005**, *106*, 843-850
- Bokros, J.C. Carbon in Medical Devices. In *Materials Science Monograph: Ceramics in Surgery*;
 P. Vincenzini (Ed.), Elsevier, Amsterdam, **1983**, *Vol. 17*, pp. 199-214.
- 10. Jenkins, G.M. Biomedical Applications of Carbons and Graphites. *Clin. Phys. Physiol. Meas.* **1980**, *1*(3), 171-194.
- 11. Kim, J.; Song, X.; Kinoshita, K.; Madou, M.; White, R. Electrochemical Studies of Carbon Films from Pyrolyzed Photoresist. *J. Electrochem. Soc.* **1998**, *145*(7), 2314-2319.

- Singh, A.; Jayaram, J.; Madou, M.; Akbar, S. Pyrolysis of Negative Photoresists to Fabricate Carbon Structures for Microelectromechanical Systems and Electrochemical Applications." J. Electrochem. Soc. 2002, 149(3), E78-E83.
- Yao, C.J.; Lai, G.M.; Chan, C.F.; Yang, Y.Y.; Liu, F.C.; Chuang, S.E. Differentiation of Pheochromocytoma PC 12 Cells Induced by Human Urine Extract and the Involvement of the Extracllular Signal-Regulated Kinase Signaling Pathway. *The Journal of Alternative and Complementary Medicine* 2005, 11(5), 903-908.
- 14. Hayat, M.A. Introduction to Biological Scanning Electron Microscopy. University Park Press, Baltimore, MD, **1978**, 131-162.
 - © 2007 by MDPI (http://www.mdpi.org). Reproduction is permitted for noncommercial purposes.